

## Design And Development Of Mucoadhesive Microspheres Of Chlorpheniramine Maleate For Nasal Delivery

Riya Pathak<sup>1</sup>, Prof. Jaideo Pandey<sup>\*2</sup>

<sup>1, 2\*</sup> Rajarshi Rananjay Singh College of Pharmacy, Amethi, Sultanpur, U.P.-227405

**\*Corresponding author:**

Prof. Jaideo Pandey

\*Head, Department of Pharmaceutics, Rajarshi Rananjay Singh College of Pharmacy, Amethi, Sultanpur, U.P., 227405

Email ID: [jaideo.p@gmail.com](mailto:jaideo.p@gmail.com)

*Cite this paper as:* Riya Pathak, Prof. Jaideo Pandey, (2025) Design And Development Of Mucoadhesive Microspheres Of Chlorpheniramine Maleate For Nasal Delivery. *Journal of Neonatal Surgery*, 14 (15s), 2446-2456.

### ABSTRACT

Drug delivery methods that allow for prolonged, close contact between the drug and the mucosa are known as mucoadhesive drug delivery systems. In order to prevent hepatic first-pass metabolism, increase residence time, and improve therapeutic efficacy, the current study aimed to produce mucoadhesive microspheres for nasal delivery. In our work, we used the Emulsification cross linking approach to create Chlorpheniramine maleate mucoadhesive microspheres with conjugation of chitosan. The microspheres were assessed in terms of their stability, in vitro drug release, in vitro mucoadhesion, percentage yield, particle size, entrapment efficiency, and swelling properties. Using SEM and FTIR technologies, microspheres were characterised. Each batch's average microsphere's particle size was found compiling with in the desired/recommended range, ensuring that every batch had appropriate handling qualities. It was discovered that the range of drug encapsulation efficiency, percentage yield & percentage for mucoadhesion for all formulations were observed to justify the recommended range. When all of the formulations were tested for In-vitro drug release using phosphate buffer 6.8 pH, microspheres showed regulated drug release for up to six hours. According to the results gathered, mucoadhesive microsphere technology represents a very promising nasal delivery for improving patient compliance and delivering medication over an extended period of time.

**Keywords:** Nasal Delivery, Mucoadhesion, Microsphere, Chlorpheniramine maleate, Chitosan, Emulsification-cross linking.

### 1. INTRODUCTION

**Nasal administration** has been used historically for both local and systemic conditions. Because of its quick absorption and potency, it is a desirable alternative to needle-based systemic drug delivery for immunizations. Furthermore, it has become well-known as a stable way to distribute drugs widely, which is particularly helpful for injectable drugs that are inefficient when taken orally because of digestive system breakdown.

**Nasal Delivery and Overcoming Challenges:** By avoiding liver metabolism, nasal administration helps to mitigate problems like sluggish absorption, low bioavailability, and drug degradation. Not for administering medication or vaccines, though; rather, it's important to remember that the nose tube serves mainly to protect the lungs from dangerous substances.

**Perks of Drug Absorption through the Nasal Cavity:** A well-vascularized epithelium, effective absorption, a porous endothelium, a large surface area, improved blood flow, and neutral pH mucus are benefits of medications absorbed through the nasal cavity. These advantages are obtained without undergoing early metabolism in the stomach or pancreas. **Chlorpheniramine Maleate** is an antihistamine used primarily to treat allergic conditions such as hay fever, rhinitis, urticaria (hives), and other allergic reactions. It works by blocking the effects of **histamine**, a substance produced by the body during an allergic response. Nasal delivery of CPM via mucoadhesive microspheres can enhance bioavailability, prolong drug residence time, and improve therapeutic efficacy by adhering to the nasal mucosa. Nasal distribution of the drug is one possible substitute delivery technique for people who have trouble swallowing, especially those who are nauseous. One strategy that has been investigated to improve drug absorption through the nasal route is the use of bio adhesive polymers. Bio adhesive polymers increase the absorption of nasal medications by extending the duration of the drug in the nasal cavity and promoting the formation of tight connections between epithelial cells. Mucoadhesive medication administration technique, particularly for usage in the nose and other mucosal areas, are made of bio adhesive polymers

known as carbomers. Using absorption enhancers, such as cyclodextrins, fusidate derivatives, fatty acids, phospholipids, surfactants, and bile salts, is another technique.

**Chitosan microspheres** are becoming more and more well-liked as efficient nasal medication delivery devices. Biocompatible, non-toxic, and biodegradable, chitosan is a polymer that adheres well to biological surfaces. Because of its amino group, it has a positive charge and is created by de-acetylating chitin. With the nasal epithelium's negatively charged mucus layer, chitosan's positive charge enables it to create robust connections.

## 2. SUPPLIES & METHODS

### Substances, Equipment, and Chemicals:

Ultra Drugs Pvt. Ltd. sent me a gift of Chlorpheniramine Maleate. The supplier of chitosan was Sisco Research Laboratories Pvt Ltd. The remaining chemicals were analytical grade and used exactly as it is, no further purification was needed. The Shimadzu Pharma Spec 1700 double-beam UV spectrophotometer, located in Kyoto, Japan, was used for the spectrophotometric studies.

### The Process of Creating Mucoadhesive Microspheres:

#### Method Of Preparation By W/O Emulsion Cross Linking Method

- Step-1: Taken a 10 ml of 2% aqueous acetic acid solution.
- Step-2: Now taken a given quantity of (0.1/0.2/0.3 gm) of chitosan was dissolved in a 10 ml of 2% aqueous acetic acid solution by continuously stirring until a homogenous solution was obtained.
- Step-3: Then added the drug (0.1 gm) slowly with stirring in prepared chitosan solution. Dispersed phase was prepared.
- Step-4: Now we prepared stabilizing agent DOSS (0.2%). Given quantity (about 50 mg) of DOSS was dissolved in 25 ml glycerine continuously stirring by glass rod.
- Step-5: Then 50 ml heavy and 50 ml light liquid paraffin was taken in 500ml pvc beaker, place under electronic stirring machine for 15 min at 1500-1600 rpm.
- Step-6: Added DOSS (stabilizing solution) as per the given quantity (2 ml or 3 ml) constant stirring at 1500-1600 rpm for 15 minutes. External Phase was prepared.
- Step-7: The dispersed phase (drug + chitosan + acetic acid) was added slowly to the above prepared external phase under constant stirring at 1500 -1600 rpm for 15 minutes.
- Step-8: Added Glutaraldehyde was added to above solution using continuously stirring for next 2 or more hours at 1500-1600 rpm.
- Step-9: Microspheres was prepared and filtered using vacuum filtration.
- Step-10: Firstly, washed with the n-hexane and then washed with the water. Kept for air drying about 24 hours and then stored in desiccator until next use.

**TABLE 1: Different Microspheres Variables:**

Formulation	PROCESS VARIABLES			CONSTANT PARAMETERS		
	Drug polymer Ratio	DOSS (ml)	GLA (ml)	Phase Ratio (Aqueous to Oil)	Stirring Rate (rpm)	Cross Linking Period (hours)
FCM1	1:1	2	2	10:100	1500 – 1600	2
FCM2	1:2	2	2			
FCM3	1:3	2	2			
FCM4	1:1	3	4			
FCM5	1:2	3	4			
FCM6	1:3	3	4			

# Mean ± Std. Deviation whereas n=3

### Characterisation of Chlorpheniramine Maleate Loaded Microspheres:

#### Particle Size:

Each microsphere was assessed in terms of its dimensions and form. The microsphere-prepared slide was inspected using an optical microscope, and the microspheres size were measured using the Olympus Master camera and modified Magnus Pro 3.0 software on the microscope (OLYMPUS). Average particle size of dried microspheres suspended in glycerine was calculated.

#### Production Yield:

By comparing the weight of the finished product after drying to the initial total weight of the medication and polymer used to make the microspheres, the percentage yield of prepared microspheres was calculated. After that, the dried microspheres were gathered and precisely weighed. Next, the formula below was used to compute the % yield. (10)

$$\% \text{ yield} = \frac{\text{Mass of microspheres obtained}}{\text{Total weight of drug and polymer}} \times 100$$

#### Entrapment Efficiency:

An ultrasonic stirrer was used to crush and dissolve an exact measurement equal to 5 mg of Chlorpheniramine Maleate microspheres in 100 ml of ethanol, which was then left overnight. Whatmann filter paper No. 41 was used to filter the final mixture. The appropriate dilutions (10, 20, 30, 40 & 50 mcg/ml) were made. By means of a UV spectrophotometer at 262 nm, the drug content of the samples was examined. The following equations (1) were used to calculate entrapment efficiency.

$$\text{Entrapment efficiency} = \frac{\text{Actual amount of drug in microspheres}}{\text{Theoretical amount of drug in microspheres}}$$

Eqn.....1

#### SEM Analysis:

Using scanning electron microscopy, the surface properties of the updated formulation (F3) were examined (JSM 6100, Jeol Ltd, Japan). Images were captured with a 100X magnification and an acceleration voltage of 10 kv.

#### FTIR Analysis for Interactions

An FTIR spectrophotometer (model – Spectrum Two, PerkinElmer, US) was used to analyse Chlorpheniramine maleate, chitosan, and the improved formulation (f3). The test sample was put into the device after being diluted with KBr until it reached a final dilution of 1:10. Measurements were made in transmittance mode against the pure KBr background spectrum, in the 400–4000 cm<sup>-1</sup>. The resolution of the instrument was set at 4cm<sup>-1</sup>, and every measurement was taken 50 times.

#### UV Spectrophotometric Studies:

Using distilled water, ethanol, and phosphate buffer with a pH of 6.8, standard curves were created for values ranging from 10 to 25 mcg/ml. Within a particular range of 261 nm, the absorbance was measured and recorded.

#### Swelling Capacity:

Precisely balance After being weighed, 50 mg microspheres (W) were incubated for 24 hours at pH 6.8 in phosphate buffer saline. Whatman filter paper was used to separate the enlarged microspheres after a 24-hour period. After gathering the microspheres and blotting them to remove extra water, their weights were recorded. It was also discovered that the swelling index depended on the particle's surface area. It was discovered that the swelling index rose along with the particle surface area.

$$\text{Swelling index} = \frac{(D_2 - D_1)}{D_1} \times 100$$

Eqn.....2

Where,

D<sub>1</sub> = Microspheres' Final Diameter after swelling.

D<sub>2</sub> = Microspheres' Initial Diameter before swelling.

#### Drug Release Studies and Research Procedures in Vitro:

The drug release investigation was conducted using the USP XXIV basket apparatus, rotating the basket at 50 rpm and 37°C

$\pm 0.5^{\circ}\text{C}$ . 900 mL of phosphate buffer with a pH of 6.8 was utilized as the dissolve media in accordance with the USP XXVI dissolving standards. Microspheres containing Chlorpheniramine Maleate (5 mg) were utilized in the experiment. The sample solution was extracted in a quantity of 5ml at predetermined intervals, passed through a Whatmann filter paper, diluted appropriately, and then analyzed using spectrophotometry. A new batch of dissolving medium was quickly added in an equivalent volume after the test sample was removed. Based on absorbance measurements at 262 nm, the percentage of medication dissolved at different time periods was computed.

#### Drug Release Mechanism and Kinetics:

Regression analysis of the afore mentioned plots was used to calculate the coefficient of correlation ( $r^2$ ) values for the linear curves in the drug release data from the in-vitro dissolution study using a variety of kinetic models, including zero order, first order, Higuchi's, Peppas's and others. This allowed for a better understanding of the mechanism and kinetics of drug release. In summary, four kinetics models of data treatment were used to plot the findings from in-vitro release investigations.

#### Stability:

For stability investigations, the formulation (FCM3) was created from the produced microspheres. Three sample sets of the formulation were separated and stored at  $4 \pm 1^{\circ}\text{C}$ ,  $25 \pm 2^{\circ}\text{C}$  &  $60 \pm 5\% \text{RH}$  and  $37 \pm 2^{\circ}\text{C}$  &  $65 \pm 5\% \text{RH}$ . After 30 days, the samples were tested for drug release. Percentage drug content for the same composition was also examined.

### 3. RESULTS & DISCUSSIONS

#### Preparation of Mucoadhesive Microsphere:

This work showed that the emulsification-cross linking approach (described below) was a suitable and simple way for loading Chlorpheniramine maleate into chitosan microspheres. A polar organic solvent was used as the "aqueous phase" to produce water-in-oil (w/o) emulsion.

#### Characterisation of Chlorpheniramine maleate loaded Mucoadhesive microspheres:

##### Size of Particle:

Table 2 displays the average particle sizes of the formulas. The microspheres had mean particle sizes ranging from 10 to 29  $\mu\text{m}$ . Mucoadhesive polymer concentration gradually affects the particle size, and stirring rate is the main factor influencing it. Regardless of polymer concentration levels, it is clear that increased stirring speeds lead to smaller particle sizes. On the other hand, there is an inverse link between particle size and mucoadhesive polymer concentration.

##### Production Yield:

The emulsion cross-linking approach produced microspheres with production yields ranging from 91.23% to 94.97%. For Chlorpheniramine maleate, as shown in Table 2. The study showed that the microspheres with a 1:3 (drug to polymer) ratio produced a higher production yield.

##### Entrapment Efficacy:

The entrapment consistently exceeded 75%, high encapsulation values. It was noted that increased drug to polymer ratios were associated with higher entrapment efficiencies.

**TABLE 2: Characterisation of Chlorpheniramine Maleate Loaded Microspheres:**

Sr. No.	Formulation Code	Particle Size ( $\mu\text{m}$ )	Production yield (%)	Encapsulation Efficiency (%)	Mucoadhesion (%)	% Drug's Content	Swelling index (%)
1.	FCM1	$29 \pm 3.98$	85.20	83.21	$60.17 \pm 0.396$	81.89	0.89
2.	FCM2	$25 \pm 4.16$	88.51	86.93	$66.17 \pm 0.431$	82.93	1.07
3.	FCM3	$20 \pm 2.01$	94.97	91.56	$71.45 \pm 0.921$	91.39	1.35
4.	FCM4	$27 \pm 2.92$	86.72	84.43	$62.72 \pm 0.325$	84.42	0.84
5.	FCM5	$26 \pm 3.51$	91.23	87.11	$67.98 \pm 0.584$	87.21	0.98
6.	FCM6	$21 \pm 1.96$	93.16	89.32	$68.87 \pm 0.123$	89.9	1.27

Mean  $\pm$  Std. Deviation whereas n=3

#### Scanning Electron Microscopy i.e SEM:

The optimized formulation, FCM3, produced spherical shaped microspheres with a smooth surface, according to SEM examination.

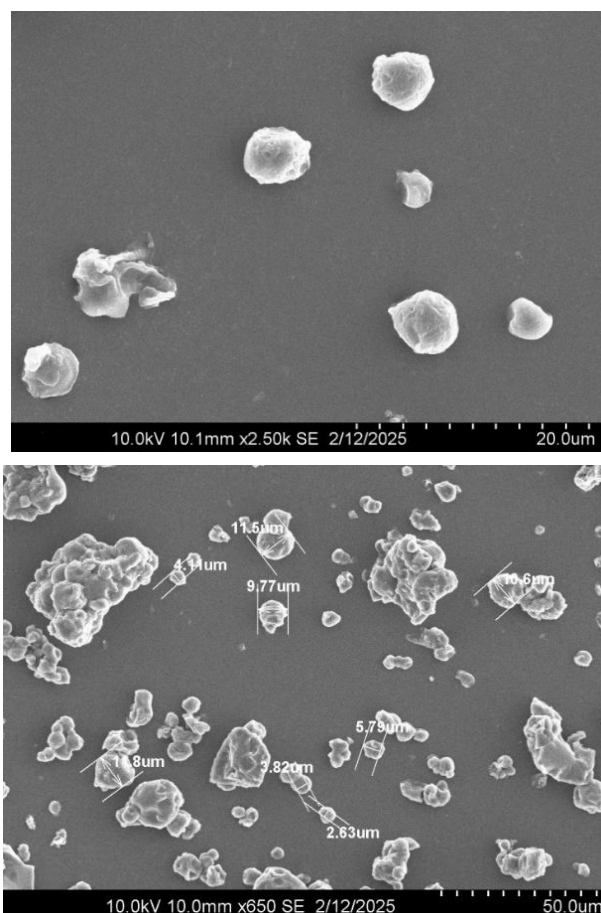


Fig. 1: FCM3's SEM

#### FTIR:

With FTIR spectroscopy, potential interactions between the crosslinking agent, chitosan, and Chlorpheniramine Maleate were investigated. The drug is preserved within the formulation and there is no drug-polymer interaction, the drug-loaded microspheres' spectrum indicated. Variations in peak intensity suggest that the drug-polymer interaction is not significant. The results of the FTIR for the FCM3 Formulation, Chlorpheniramine Maleate and Chitosan are displayed below as Figures 2, 3, and 4 respectively.

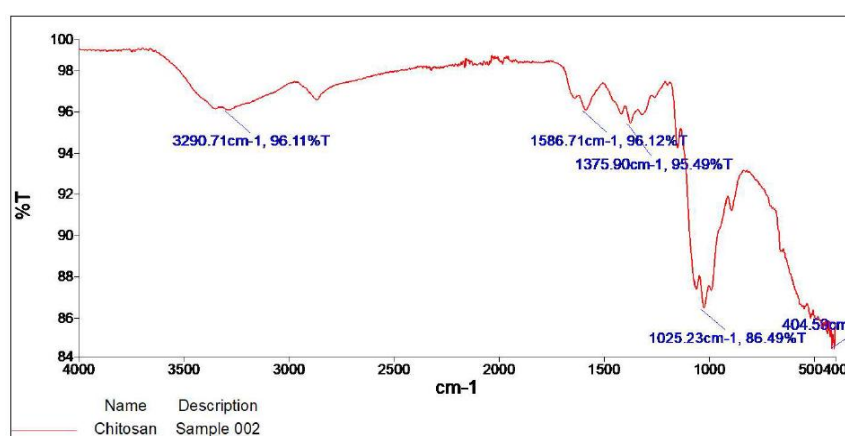


Fig. 2: FTIR of Chitosan

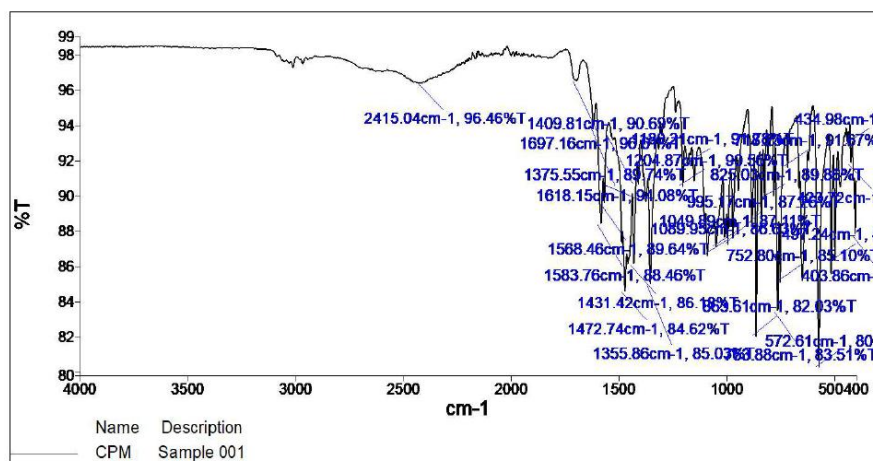


Fig. 3: Pure Drug Chlorpheniramine Maleate's FTIR

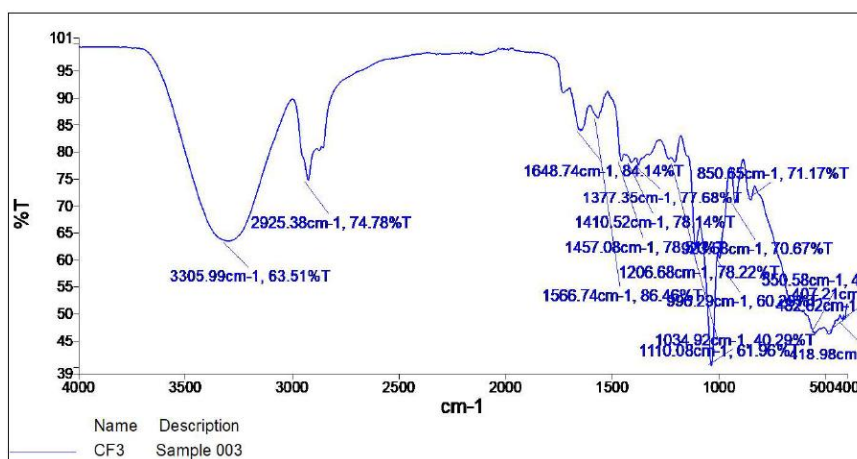


Fig. 4: FCM3's FTIR

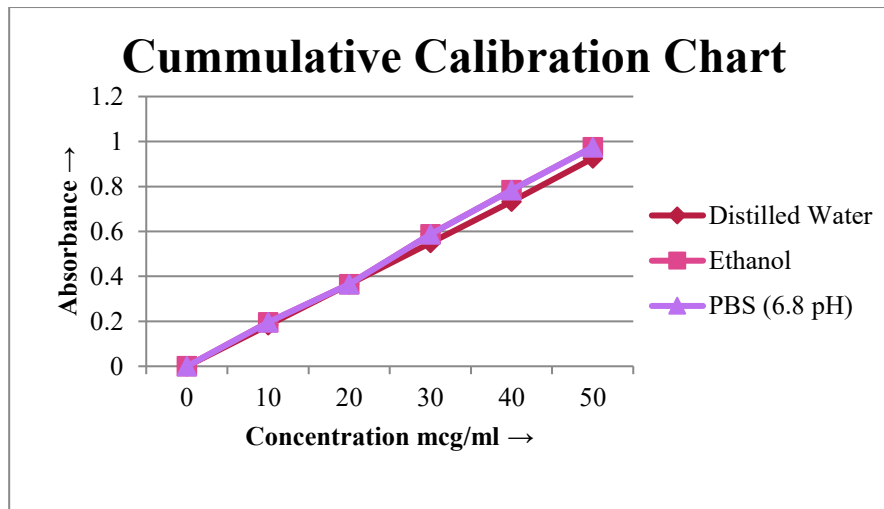
#### Assessment of Pure API by UV Spectrophotometre:

By following the application of Beer-Lambert's Law over the concentration range of 10–50 µg/ml and using three different solvents - distilled water, ethanol and phosphate buffer with a pH of 6.8 the absorbance at 262 nm was measured (table 3) and calibration curves were produced (figure 5).

TABLE 3: STANDARD CALIBRATION OF CHLORPHENIRAMINE MALEATE:

Sr. No.	Concentration (µg/ml)	Absorbance		
		Distilled Water	Ethanol	Phosphate Buffer (6.8 pH)
1.	10	0.183	0.195	0.257
2.	20	0.365	0.365	0.502
3.	30	0.548	0.587	0.769
4.	40	0.732	0.783	1.021
5.	50	0.925	0.975	1.277
R <sup>2</sup> Value		0.9999	0.9992	0.9998

Mean ± Std. Deviation whereas n=3



**Fig. 5: Cumulative Calibration Curve for Pure Chlorpheniramine maleate in Different Solvents.**

#### Swelling Ability of Microspheres Prepared:

Table 2 displays the swelling index for each formulation. The microspheres' degree of swelling varied amongst formulations, ranging from 0.84% to 1.35%. It is noted that as mucoadhesive polymer concentrations rise, the degree of swelling tends to significantly increase.

#### In-Vitro Mucoadhesion:

Based on polymer content, the mucoadhesion of nasal microspheres loaded with Chlorpheniramine Maleate varied from  $60.17 \pm 0.396\%$  to  $71.45 \pm 0.921\%$  (Table 2).

#### In-Vitro Release Investigations:

Table 4 provided an overview of each formulation's in vitro release profiles. Figure 6 shows the release characteristics of chitosan microspheres loaded with Chlorpheniramine Maleate. It became evident that the polymer concentration and stirring rate had a big influence on the drug's release.

**TABLE 4: In-Vitro Drug Release of Pure CHLORPHENIRAMINE MALEATE & Formulations of Microspheres loaded with DRUG:**

Time in Hours	Cumulative % drug release $\pm$ SD						
	Pure drug	FCM1	FCM2	FCM3	FCM4	FCM5	FCM6
0	0	0	0	0	0	0	0
0.5	3.27	4.87	6.34	9.46	7.17	8.45	8.73
1	10.92	14.47	17.13	20.53	15.68	18.03	18.95
2	18.65	23.23	25.43	34.17	26.41	27.53	31.67
3	25.78	34.54	38.36	43.56	34.99	36.51	40.47
4	32.83	44.77	48.72	53.63	45.82	47.11	49.93
5	55.98	60.69	64.97	72.89	61.79	63.54	66.31
6	64.13	73.26	79.56	89.69	75.63	78.05	84.23

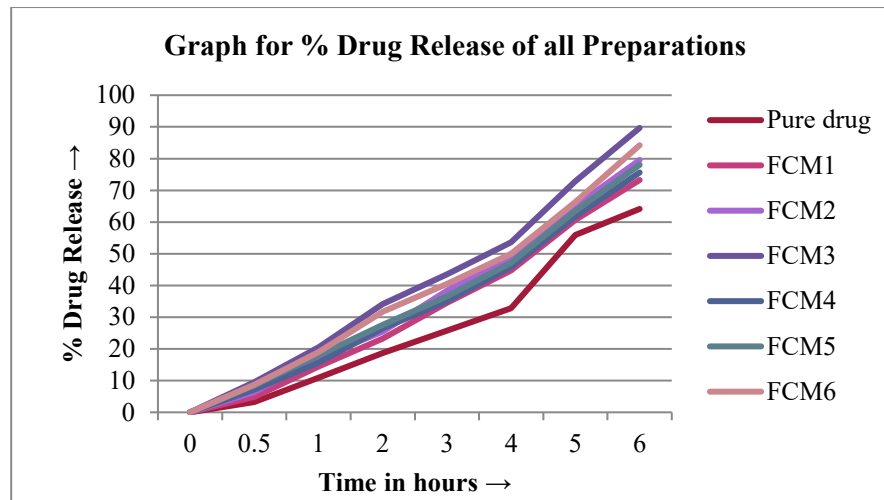


Fig. 6: In-Vitro Drug Release of All 6 Formulations

#### Drug Release Kinetic Studies in Vitro Using Different Models:

The Higuchi Equation, the Korsmeyer-Peppas model, the Zero-order, and the First-order models were used to analyze the in vitro drug release properties of each formulation. Table 5 displays the outcomes.

TABLE 5: The diffusion coefficient (N) values of the Peppas equation and regression coefficient ( $r^2$ ) values, used in the analysis of microspheric release data according to different kinetic models.

Formula code	Zero order	First order	Higuchi's	Korsmeyer-Peppas	
	R	R	R	n	R
FCM1	0.9656	0.9492	0.9653	0.6254	0.9744
FCM2	0.9678	0.9802	0.9673	0.6575	0.9836
FCM3	0.9887	0.9838	0.9844	0.6644	0.9892
FCM4	0.9732	0.9738	0.9793	0.6378	0.9797
FCM5	0.9757	0.9766	0.9811	0.6456	0.9804
FCM6	0.9798	0.9816	0.9834	0.6623	0.9884

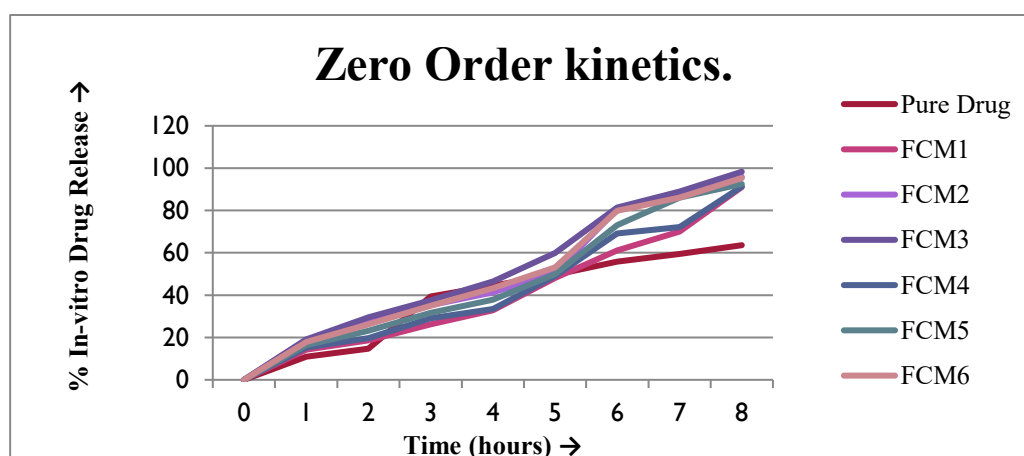


Fig. 7: Chlorpheniramine Maleate Microsphere Formulations: Zero Order Release Kinetics.

### Stability Assessment of Chlorpheniramine Maleate Microspheres:

For the purpose of evaluating the stability of the formulated Chlorpheniramine Maleate microspheres, the ideal formulation FCM3 was stored for six months under the following conditions:  $4\pm1^{\circ}\text{C}$ ,  $25\pm2^{\circ}\text{C}$  with  $60\pm5\%$  RH, and  $37\pm2^{\circ}\text{C}$  with  $65\pm5\%$  RH displayed in Table 6. It's interesting to note that formulations kept at  $25\pm2^{\circ}\text{C}$  with  $60\pm5\%$  RH showed the highest percentage levels of entrapment, followed by formulations kept at  $4\pm1^{\circ}\text{C}$  and  $37\pm2^{\circ}\text{C}$  with  $65\pm5\%$  RH conditions. These findings may be explained by the facts that point to a partial erosion of the polymer matrix during storage.

**TABLE 6: STABILITY STUDIES OF FCM3, THE OPTIMISED FORMULATION:**

Sr. No.	Time Months	in $4\pm1^{\circ}\text{C}$		$25\pm2^{\circ}\text{C}$ with $60\pm5\%$ RH		$37\pm2^{\circ}\text{C}$ with $65\pm5\%$ RH	
		Z	Y	Z	Y	Z	Y
1	1	85.9	84	85.9	84.05	85.93	84.03
2	2	85.8	83.6	85.8	84.03	85.62	84.01
3	3	85.7	83.6	85.7	84	85.1	83
4	4	85.0	83.5	85.5	83.9	84.7	82.8
5	5	84.7	83.4	85.3	83.8	84.3	82.5

# Z= % Entrapment Efficacy & Y= % Cumulative Drug Release

### 4. CONCLUSION

It is clear from the ongoing studies that Chlorpheniramine Maleate microspheres, which are made with chitosan using emulsification cross-linking technique, have potential for use in nasal delivery. As a result, the created microsphere becomes a potential candidate for an intranasal controlled medication delivery system.

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